

ARAPLBS: Robust and efficient elasticity-based optimization of Weights and Skeleton Joints for Linear Blend Skinning with Parameterized Bones – Additional Material – Spines for linear blend skinning transformations

J.-M. Thiery^{1,2†}

E. Eisemann^{1‡}

¹Deft University of Technology, The Netherlands ²LTCI, Telecom-ParisTech, Université Paris-Saclay, Paris, France

Abstract

In this document, we present the formulas for the transformation of 3d points via spines, a new type of deformer, in the context of linear-blend-skinning transformations. A spine is initially defined as a straight bone, which is virtually subdivided into an infinity of sub-bones, which are then all transformed in the same way. The name of this deformer hints at its use as a spine for 3D models. Compared with traditional rigid bones for LBS, whose parameters are a rotation and translation, a spine deformer has three additional control parameters: a roll axis, a roll amount, and a stretch value.

1. Important notes

For convenience, this document also contains the related parts of the main article [TE17]. The derivation, which was left out of the paper, is described in this document in Sec. 4.

If you are using the following work, please cite the main article: [TE17].

2. Linear Blend Skinning (LBS) with parameterized bones

The location of a vertex i under LBS [MTLT*88, LCF00], using *parameterized bones*, is given by

$$f : v_i \mapsto \sum_{j \in B(i)} w_{ij} (R_j(v_i) \cdot v_i + T_j(v_i)), \quad (1)$$

where $R_j(v_i)$ is the rotation and $T_j(v_i)$ the translation applied by bone j on vertex i (these are constant for rigid bones – $(R_j(v_i), T_j(v_i)) = (R_j, T_j) \forall i$, but depend on v_i otherwise), $B(i)$ is the set of bones influencing i and w_{ij} the *weight* of

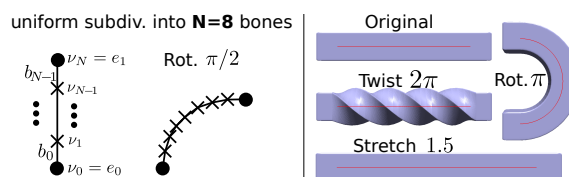


Figure 1: **Left:** Approximation. **Right:** Continuous setting.

bone j over i . We will refer to $\{B(i)\}$ as the *bone influence maps* and to $\{w_{ij}\}$ as the *weight maps*.

Typically, skinning weights should verify:

1. **Affinity:** $\sum_j w_{ij} = 1$; reproduces rigid transformations.
2. **Positivity:** $w_{ij} \geq 0$; prevents unnatural behavior.
3. **Sparsity:** only “few” $w_{ij} > 0$; leads to “simpler” controls and a faster rendering process (*ill-defined*).
4. **Locality:** bones should have “small” influence zones; improves control over editing operations (*ill-defined*).

3. Spines

An example of parameterized bones are TSBs [JS11]. Our approach is compatible with these, as well as a generaliza-

[†] jean-marc.thiery@telecom-paristech.fr

[‡] e.eisemann@tudelft.nl

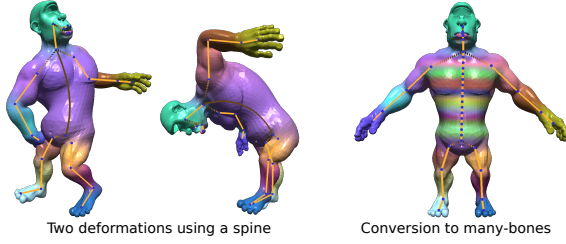


Figure 2: Conversion of spines to many-bones. **Left:** deformations using a spine for the torso. **Right:** Converting the spine to 16 bones and their weight maps.

tion, *spines*, described here. A *spine* \mathbf{s} is a skeletal segment $[e_0, e_1]$ subdivided into infinitely-small bones undergoing the same transformation (Fig. 1). The name reflects its suitability to represent spines in models. Fixing e_0 , its transformation combines a stretch σ_s , affecting its length, and a rotation around an axis a_s , such that the accumulated rotation from e_0 to e_1 amounts to θ_s . Similar to other bones, a spine \mathbf{s} also has a rigid transformation applied to e_0 , the *spine's base transformation* (R_s, t_s) . In consequence, spines have 5 parameters: $(R_s, t_s, \sigma_s, \theta_s, a_s)$, and TSBs are twist-restricted spines (i. e., $a_s = \overrightarrow{e_0 e_1} / \|\overrightarrow{e_0 e_1}\|$ in their case).

A point p with parameter $u_p \in [0, 1]$ (describing “which small bone” p is attached to) is transformed by a spine as

$$p \mapsto R_s R_{\text{loc}}(u_p) \cdot p + R_s t_{\text{loc}}(u_p) + t_s, \text{ with} \quad (2)$$

$$R_{\text{loc}}(u) := \text{Rot}(a_s, u\theta_s), \text{ and} \quad (3)$$

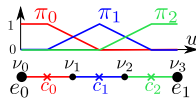
$$t_{\text{loc}}(u) := (\text{Id} - R_{\text{loc}}(u)) \cdot e_0 + \sigma_s \cdot (\sin(u\theta_s) / \theta - u \cos(u\theta_s)) (\text{Id} - a_s \cdot a_s^T) \cdot \overrightarrow{e_0 e_1} + \sigma_s \cdot (u \sin(u\theta_s) + (\cos(u\theta_s) - 1) / \theta_s) a_s \times \overrightarrow{e_0 e_1} + u \cdot (\sigma_s - 1) R_{\text{loc}}(u) \cdot \overrightarrow{e_0 e_1}. \quad (4)$$

3.1. Mesh parameterization

Given a spine \mathbf{s} with vertices e_0, e_1 , one needs to define the above parametrization $u_s : \mathcal{V} \mapsto [0, 1]$ on the mesh vertices \mathcal{V} . It is possible to use complex (or artistically-driven) definitions [JS11], but by default, we use a linear parameterization: $u_s(v_i) = \max(0, \min(1, \overrightarrow{e_0 v_i}^T \cdot \overrightarrow{e_0 e_1} / \|\overrightarrow{e_0 e_1}\|^2))$.

3.2. Conversion of spines to many-bones

If a system only supports rigid bones, \mathbf{s} can be converted into a set of them: \mathbf{s} is cut into n bones with joints $v_0 \cdots v_n$ and for each v_j its corresponding u -parameter u_j is determined. We define a unity partition as piecewise-linear functions $\{\pi_j : [0, 1] \mapsto [0, 1]\}$, where $\pi_j(c_k) = \delta_j^k$, with $c_j = (u_j + u_{j+1})/2$, and impose $\pi_0(0) = \pi_n(1) = 1$ (the inset shows the case for 3 bones). The weight of a mesh vertex v_i (with weight w_{is} w.r.t. the spine) w.r.t. bone k is defined as $w_{ik} \pi_k(u_s(v_i))$.



3.3. Jacobians

The Jacobian of a normal bone is simply its rotation. For a parameterized bone with transformation given by Eq. 2, its Jacobian at point p with parameter $u(p)$ is

$$J_p = R_s \left(R_{\text{loc}}(u_p) + (R'_{\text{loc}}(u_p) \cdot p + t'_{\text{loc}}(u_p)) \cdot \overrightarrow{\nabla} u(p) \right) \quad (5)$$

In Eq. 5, $\overrightarrow{\nabla} u(p)$ is needed. Our work uses a linear parametrization, which is not differentiable at $u = 0$ and 1. Moreover, such parameterizations are generally defined on the mesh only (e. g., hand-painted, or resulting from a diffusion on the mesh), and their gradients do not have a closed-form expression. We thus estimate the gradient $\overrightarrow{\nabla} u_i$ at vertex i (while keeping it aligned with the bone) as

$$\overrightarrow{\nabla} u_i := \underset{g \mid g \times \overrightarrow{e_0 e_1} = \vec{0}}{\text{argmin}} \sum_{k \in V_1(i)} \lambda_{ik} \|g^T \cdot e_{ik} - (u(v_k) - u(v_i))\|^2$$

Noting $a_{s[\times]}$ the 3×3 -matrix such that $a_{s[\times]} \cdot v = a_s \times v$, $\forall v \in \mathbb{R}^3$, the derivatives of $R_{\text{loc}}(u)$ and $t_{\text{loc}}(u)$ are given by:

$$R'_{\text{loc}}(u) = \theta_s \cos(u\theta_s) a_{s[\times]} + \theta_s \sin(u\theta_s) (a_s \cdot a_s^T - \text{Id})$$

$$t'_{\text{loc}}(u) = -R'_{\text{loc}}(u) \cdot e_0 + \sigma_s \cdot (\cos(u\theta_s) + u\theta_s \sin(u\theta_s)) (\text{Id} - a_s \cdot a_s^T) \cdot \overrightarrow{e_0 e_1} + \sigma_s \cdot (u\theta_s \cos(u\theta_s) - \sin(u\theta_s)) a_s \times \overrightarrow{e_0 e_1} + (\sigma_s - 1) R_{\text{loc}}(u) \cdot \overrightarrow{e_0 e_1} + u \cdot (\sigma_s - 1) R'_{\text{loc}}(u) \cdot \overrightarrow{e_0 e_1}.$$

4. Local transformation by a Spine

Here, we first derive the *local* transformation $(R_{\text{loc}}(u), t_{\text{loc}}(u))$ of a spine (where local implies that e_0 is fixed). Initially, we will investigate the case, where the spine is subdivided into N subsegments, which all undergo the same local rotation of axis \mathbf{a} , angle θ/N (hereby, the accumulated rotation at e_1 is θ), and a stretch σ in the direction of the spine. In this formulation, bone i links vertices v_i and v_{i+1} . Induced by the preceding bones of the spine, it undergoes a global transformation given by the stretch in direction $\overrightarrow{e_0 e_1}$, as well as a rotation R_i , and a translation t_i (i. e., $p \mapsto R_i \cdot p + t_i$). Finally, we will express the rigid transformation along the segment at a parameter $u \in [0, 1]$ via a rotation $R_{\text{loc}}(u)$ and a translation $t_{\text{loc}}(u)$ by considering the limit for $N \rightarrow \infty$: $((R_{\text{loc}}(u), t_{\text{loc}}(u)) = \lim_{N \rightarrow \infty} (R_{[u/N]}, t_{[u/N]}))$.

In a first step, we notice that

$$R_{\text{loc}}(u) = \text{Rot}(\mathbf{a}, u\theta)$$

We note \bar{p} the transformation induced by the stretch at point p with parameter u : $\bar{p} = p + u(\sigma - 1)\overrightarrow{e_0 e_1}$.

The final transformation can be obtained by first stretching the space in the spine direction (given by $p \mapsto \bar{p}$), and then applying the transformation of the stretched spine on the stretched space (which we note $\bar{p} \mapsto R_{\text{loc}}(u) \cdot \bar{p} + t_{\text{loc}}^{str}(\sigma)(u)$).

Regarding the latter, one can check by recurrence that: $t_i^{str(\sigma)} = \sum_{k=1}^i [R_{loc}((k-1)/N) - R_{loc}(k/N)] \cdot \bar{v}_k$, (since bones $k-1$ and k both transform \bar{v}_k similarly, i. e., $R_k \bar{v}_k + t_k^{str(\sigma)} = R_{k-1} \bar{v}_k + t_{k-1}^{str(\sigma)}$), and that $t_0^{str(\sigma)} = 0$, which, when using $\bar{v}(x) = e_0 + x\sigma e_0 \bar{e}_1$ and taking the limit, gives:

$$t_{loc}^{str(\sigma)}(u) = \int_{x=0}^u \frac{-dR_{loc}}{dx}(x) dx \cdot e_0 + \sigma \int_{x=0}^u -x \frac{dR_{loc}}{dx}(x) dx \cdot \bar{e}_0 \bar{e}_1$$

By decomposing the rotation matrix $R_{loc}(x) = Rot(\mathbf{a}, x\theta)$ as $R_{loc}(x) = \cos(x\theta)\text{Id} + \sin(x\theta)\mathbf{a}_{[\times]} + (1 - \cos(x\theta))\mathbf{a} \cdot \mathbf{a}^T$ using Rodrigues' formula, we obtain

$$\begin{aligned} t_{loc}^{str(\sigma)}(u) = & (\text{Id} - R_{loc}(u)) \cdot e_0 + \\ & \sigma \cdot (\sin(u\theta)/\theta - u \cos(u\theta)) \left(\text{Id} - \mathbf{a} \cdot \mathbf{a}^T \right) \cdot \bar{e}_0 \bar{e}_1 + \\ & \sigma \cdot (u \sin(u\theta) + (\cos(u\theta) - 1)/\theta) \mathbf{a} \times \bar{e}_0 \bar{e}_1 \end{aligned}$$

Since the final transformation is the composition of the stretch and the transformation by the stretched spine on the stretched space (first stretch, then rotate) (i. e., $p \mapsto R_{loc}(u) \cdot \bar{p} + t_{loc}^{str(\sigma)}(u) = R(u)_{loc} \cdot (p + u(\sigma - 1)e_0 \bar{e}_1) + t_{loc}^{str(\sigma)}(u)$), we finally obtain

$$t_{loc}(u) = t_{loc}^{str(\sigma)}(u) + u \cdot (\sigma - 1) R_{loc}(u) \cdot \bar{e}_0 \bar{e}_1$$

Note that, although not strictly defined for $\theta = 0$, the terms involving θ tend to 0 when θ tends to 0.

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